

## **Supporting Information**

# **Cell Isolation and Recovery Using Hollow Glass Microspheres Coated with Nanolayered Films for Applications in Resource-limited Settings**

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### **Biotin modification of ALG**

Alginate was conjugated with biotin hydrazide (Sigma B7639) using a standard carbodiimide reaction, as described in previous literatures.<sup>1,2</sup> Briefly, ALG was dissolved in pH 6.1 MES buffer to form a 1.0 wt.% solution. Per 50 mL of ALG solution, 80 mg of biotin hydrazide, 360 mg of 1-ethyl-3-[3-dimethylaminopropyl] carbodiimide hydrochloride (EDC, Pierce 22980), and 204 mg of hydroxysulfosuccinimide (Sulfo-NHS, Pierce 24510) were added and reacted for 3 h, after which time the solution was dialyzed against deionized water for 48 h and lyophilized.

### **Modification of PAH with fluorescein**

PAH (214 mg) was dissolved in pH 7.4 Phosphate-buffered saline (PBS) solution (4.3 mL) and placed in ice bath with stirring. Fluorescein NHS ester (10 mg) was dissolved in Dimethylformamide (DMF) (500  $\mu$ L) and added dropwise into the stirring PAH solution. After 3 h, the reaction solution was dialyzed against deionized water for 48 h and lyophilized.

### **Buoyancy force calculation**

For the hollow glass microspheres to be able to lift the cancer cell upwards, the following condition should be fulfilled:

$$F - G > 0 \quad (1)$$

$$F = \frac{4}{3}\pi \times (R_{cell}^3 + R_{HGMS}^3) \times \rho_{water} \quad (2)$$

$$G = \frac{4}{3}\pi \times R_{cell}^3 \times \rho_{cell} + \frac{4}{3}\pi \times R_{HGMS}^3 \times \rho_{HGMS} \quad (3)$$

Where F is the total buoyancy and G is the total gravity of cell and HGMS. The density of cancer cell and HGMS are 1.08 g/ml and 0.47 g/ml, respectively.<sup>3</sup>

### **Shear stress calculation**

For a solid sphere flow through a stationary liquid with uniform velocity U, the shear stress at the sphere surface can be calculated as following:<sup>4</sup>

$$\tau_{\theta} = -\frac{3}{2}\frac{\mu U}{R} \sin\theta \quad (4)$$

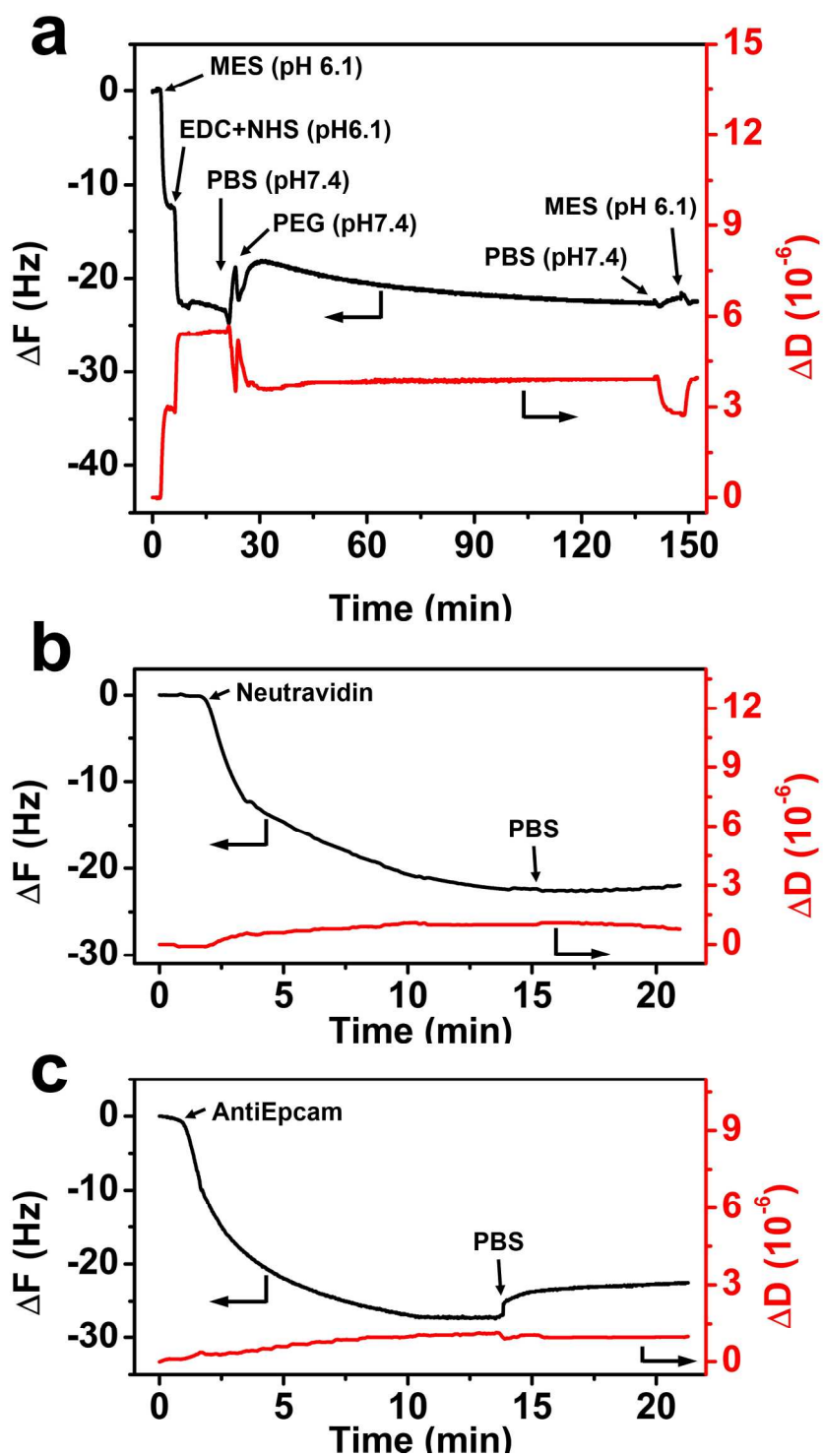
Where  $\tau_\theta$  is shear stress at angle  $\theta$ ;  $\mu$  is viscosity of the liquid;  $R$  is radius of the sphere;  $\theta$  is azimuth angle in Spherical coordinate.

The  $\mu$  of water at 20 °C is 0.001 Pa•S and  $R$  of PC-3 cell is approximate 7  $\mu\text{m}$ . A velocity ( $U$ ) of 0.001 m/s was measured in experiment. The above values were substituted into the equation (4) and the maxima shear stress of 0.21 Pa was obtained at  $\theta = \pi/2$ . This value is comparable with shear stress (0.1-1 Pa) in microfluidic devices.<sup>5,6</sup>

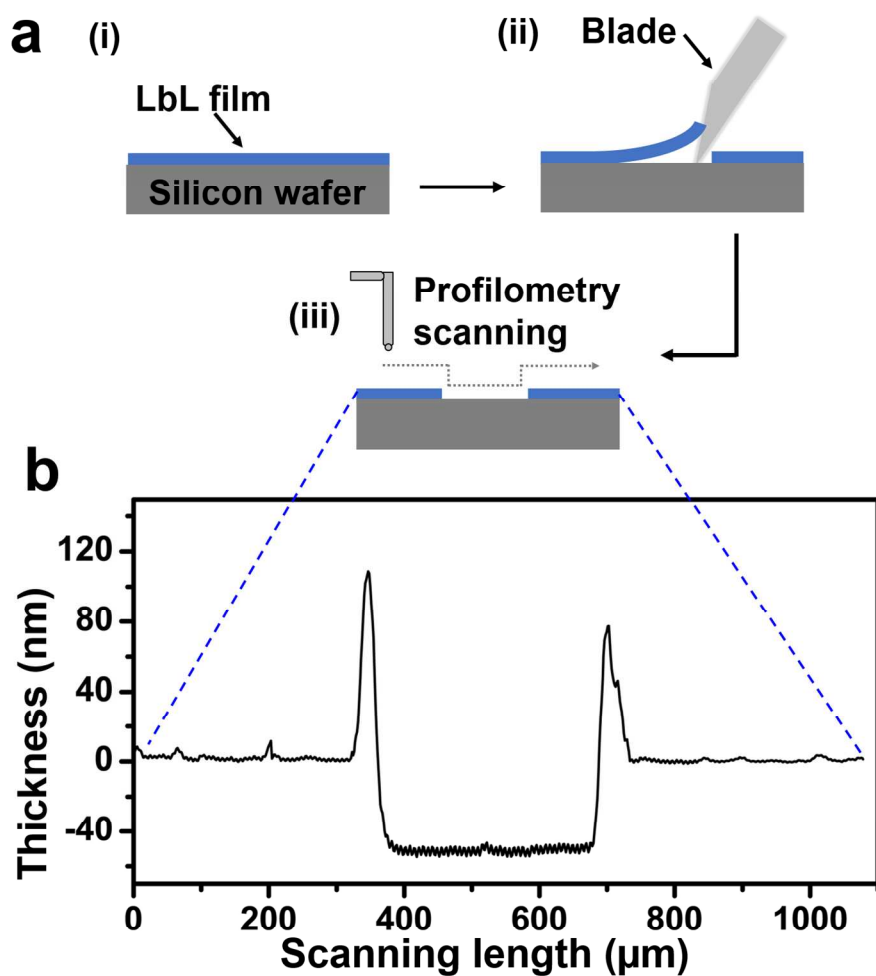
### **Film stability test**

Film stability test was performed by incubating PARG/ALG-PEG-anti-EpCAM film with blood plasma for 3 h. Similar to our previous work,<sup>6</sup> 5 bilayers of PARG/ALG films were deposited along the walls and floor of microfluidic channels formed by bonding a polydimethylsiloxane (PDMS) mold to an oxygen plasma treated glass slide.  $\text{NH}_2$ -PEG/  $\text{NH}_2$ -PEG-biotin was then modified on the film by EDC chemistry. Texas Red-labeled Neutravidin was used to conjugate biotin-anti-EpCAM onto PEG-biotin on the film. The prepared film was ready for stability test as PARG/ALG-PEG-anti-EpCAM film. Human blood was centrifuged at 300 g for 5 min to sink down all the blood cells and supernatant was kept as blood plasma. Right after the blood plasma was introduced to the PARG/ALG-PEG-anti-EpCAM film, optical fluorescent images were taken by an Olympus BX53 fluorescence microscope with 200 ms exposure time for 3 h. The result images were analyzed by ImageJ.

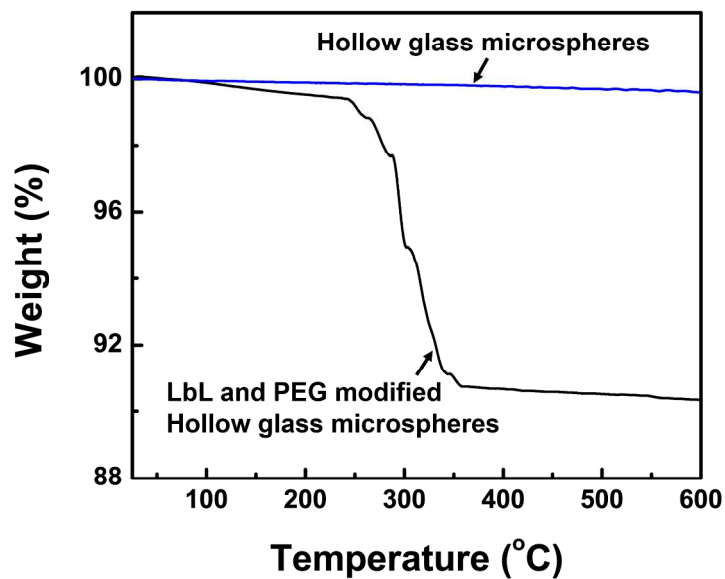
### **Supplementary Figures**



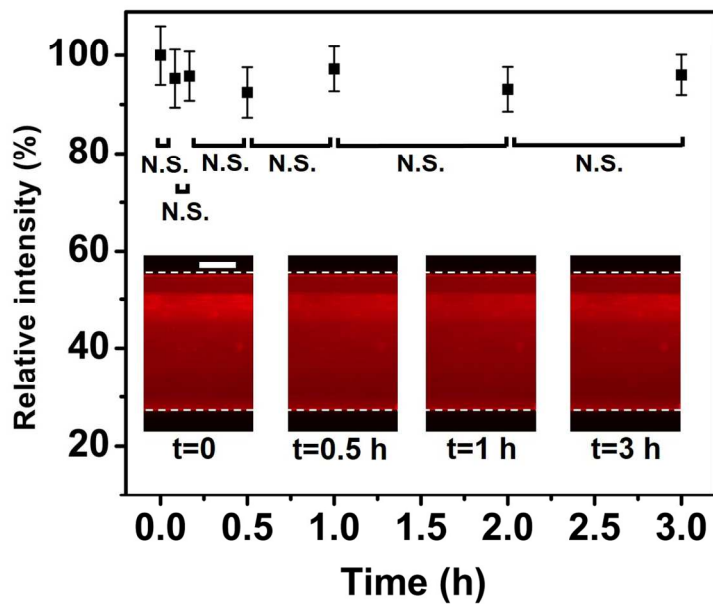
**Fig. S1.** QCM-D monitoring of surface modifications: a.  $\text{NH}_2\text{-PEG}/\text{NH}_2\text{-PEG-Biotin}$  conjugation via EDC chemistry; b. Neutravidin modification; c. antiEpCAM modification.



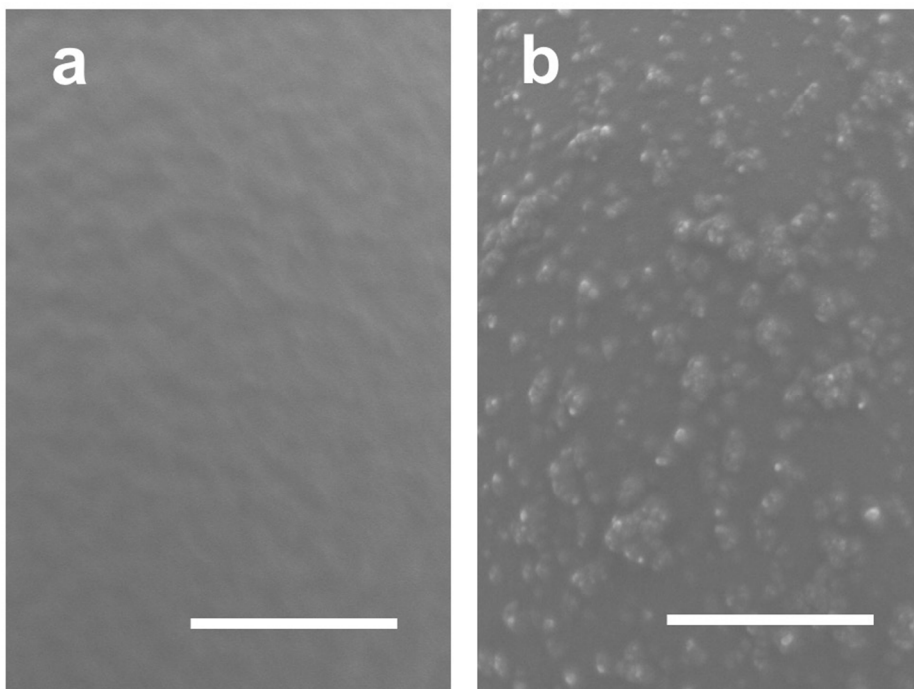
**Fig. S2.** Film thickness measurement by profilometry: a. (i) prepare LbL film on silicon wafers; (ii) scratch LbL film all the way to the silicon to form a gap; (iii) scan the gap by profilometry to get film thickness; b. profilometry result of 5 bilayer PARG/ALG on silicon wafer.



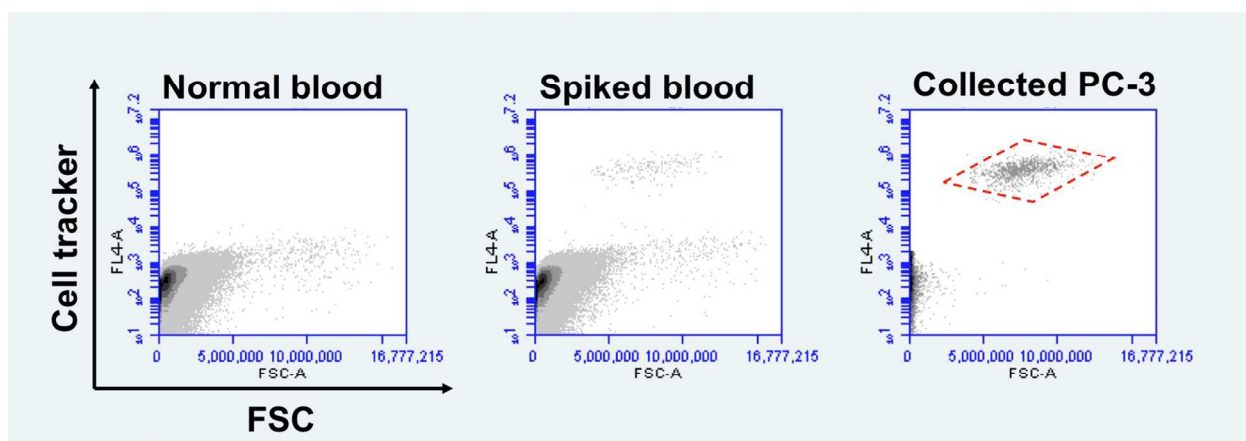
**Fig. S3.** TGA characterization of nanolayer modified and unmodified hollow glass microspheres.



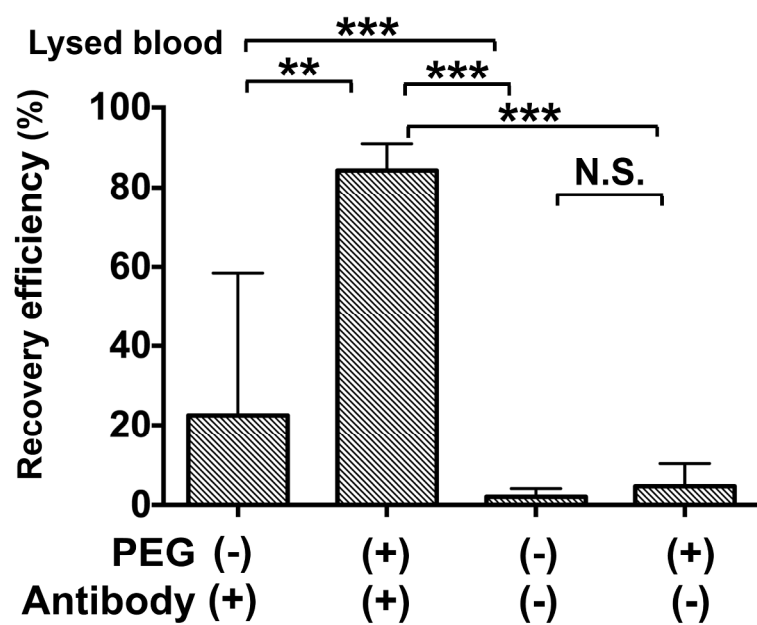
**Fig. S4.** Stability of antibody modified LbL film: Optical fluorescent images of Texas Red labeled PARG/ALG-PEG-anti-EpCAM films after being incubated for various times in blood plasma. Film edges are marked by a white dashed line. Scale is 100  $\mu$ m.



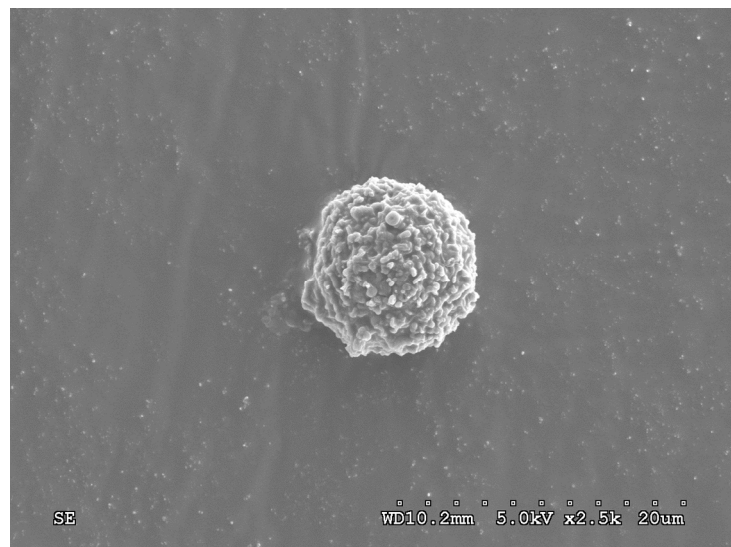
**Fig. S5.** SEM images of surface of the HGMS before (a) and after (b) cell capture and release process. Scale is 2 μm.



**Fig. S6.** Typical flow cytometry results normal blood, spiked blood and PC-3 cell recovered from blood.



**Fig. S7.** Capture and release of PC-3 from lysed blood.



**Fig. S8.** SEM image of a PC-3 cell.



## References:

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